IN THE SPECIFICATION

Please replace the paragraph beginning on page 34, line 1 (para. 155 of corresponding U.S. Publication No. 2005/0119648 A1) with the following rewritten paragraph:

The specific size and shape of the tissue engagement device 602 will, of course, depend on the intended application, as will the choice of materials. Although the present inventions are not limited to any particular sizes, shapes or materials, one exemplary implementation that is especially well suited for cardiac treatment is described hereafter. The exemplary tissue engagement device 602 cup-shaped and is formed, preferably by molding, from a soft, flexible biocompatible material such as silicone rubber or urethane. The diameter of the tissue engagement device 602 may range from about 2 mm to about 5 mm and is about 2-3 mm in the exemplary embodiment. With respect to the electrical connection of the stimulation electrodes 604 to the tissue stimulation apparatus 300, the stimulation electrodes in the exemplary implementation are carried on an outer peripheral or distal portion of the tissue engagement device 602 such that they are not located within an inner space defined by the tissue engagement device 602. The stimulation electrodes are connected to signal lines 608 that extend from the stimulation electrodes, though a shaft lumen 610, and an opening (not shown) at the proximal end of the shaft 606. The signal lines are connected to the connectors 302 on the stimulation apparatus 300 in the manner discussed above.

Please replace the paragraph beginning on page 34, line 17 (para. 156 of corresponding U.S. Publication No. 2005/0119648 A1) with the following rewritten paragraph:

In the exemplary implementations illustrated in FIGS. 25-32, the stimulation electrodes 604 are essentially the same as the stimulation and sensing electrodes 426 and 428 described above. For example, the electrodes 604 may be relatively small, low profile devices (e.g. about 0.5 mm to 1 mm in diameter and about 0.01 mm thick) that can be formed by coating one of the suitable conductive materials described above onto the tissue engagement device 602. In the illustrated embodiment, the electrodes 604 are discrete electrodes that do not extend around the peripheral sealing surface of the tissue engagement device 602.

Please replace the paragraph beginning on page 36, line 28 (para. 163 of corresponding U.S. Publication No. 2005/0119648 A1) with the following rewritten paragraph:

Another surgical tissue stimulation and sensing system, which is generally represented by reference numeral 50 in FIG. 29 includes a tissue stimulation apparatus 300, a suction source 402 and a tissue stimulation and sensing probe 616. The tissue stimulation apparatus 300 and a suction source 402 are described above. The exemplary tissue stimulation and sensing probe 616 includes a suction device 618 that carries a pair of stimulation electrodes 604 on a peripheral or distal portion of the suction device 618 such that the stimulation electrodes 604 are not located within an inner space defined by the suction device 618. The suction device ~~and~~ is supported on the distal end of a flexible tube 620. The proximal end of the flexible tube 620 is connected to a handle 622. The suction device 616 is connected to the suction source 402 by way of a lumen 624 that extends through the flexible tube 620 and a flexible tube 406 that is connected to the proximal end of the handle 622 by a connector 626 such as, for example, the illustrated Luer connector. When the suction source 402 is actuated, the suction device 602 will fix the stimulation electrodes 604 against the target tissue.